



MRI DEMO SESSION: BASICS OF NMR

Thanh Phong LÊ
CIBM MRI EPFL AIT

PHYS-473 MRI Practicals on CIBM preclinical imaging systems, 17 September 2024



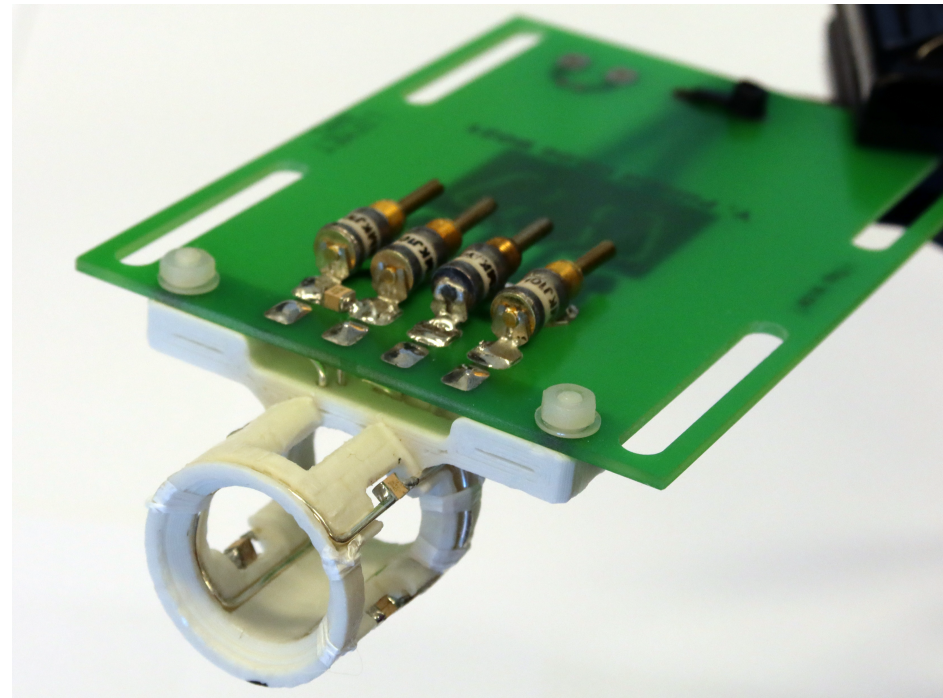
C I B M . C H

DEMO SESSION

- Overview hardware, upstairs, downstairs
 - MRI Cabinet
 - Faraday Cage
 - Magnet
- Illustration of magnetic field and eddy current

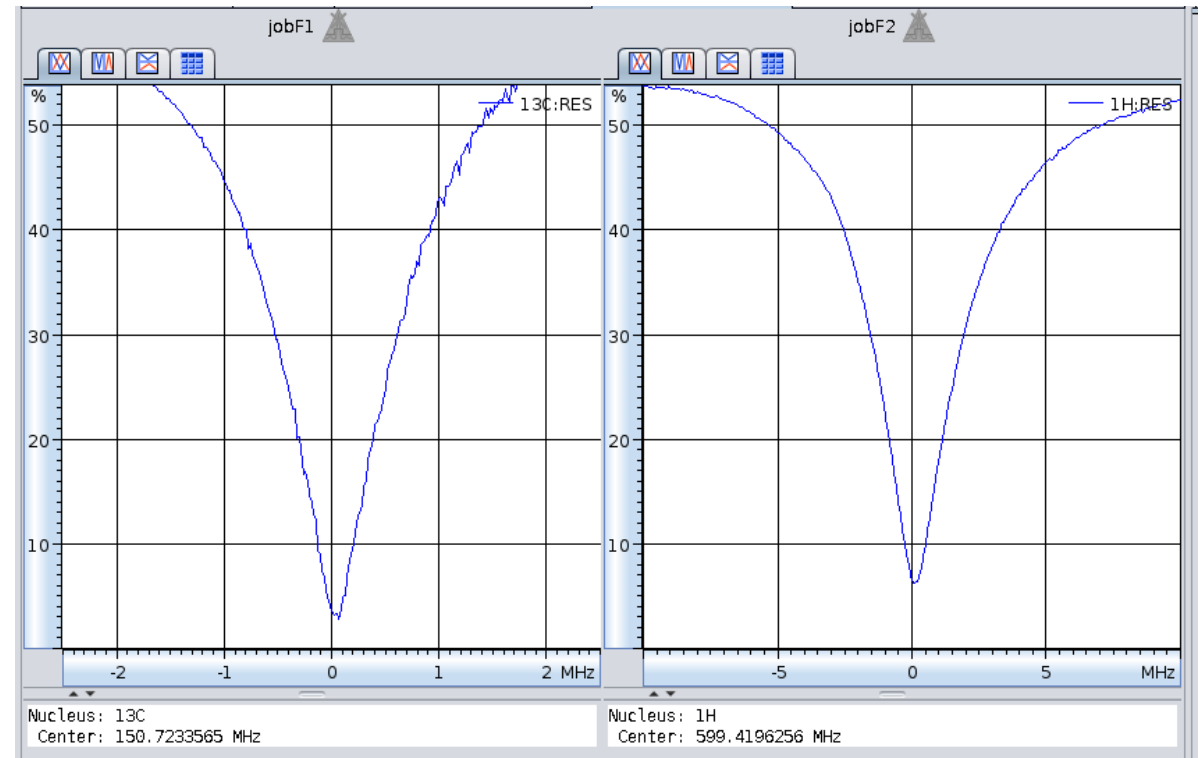
DEMO SESSION

- Sample: 1g/L CuSO_4 in H_2O .
- Coil: $^1\text{H}/^{13}\text{C}$ saddle coil (18mm ID)



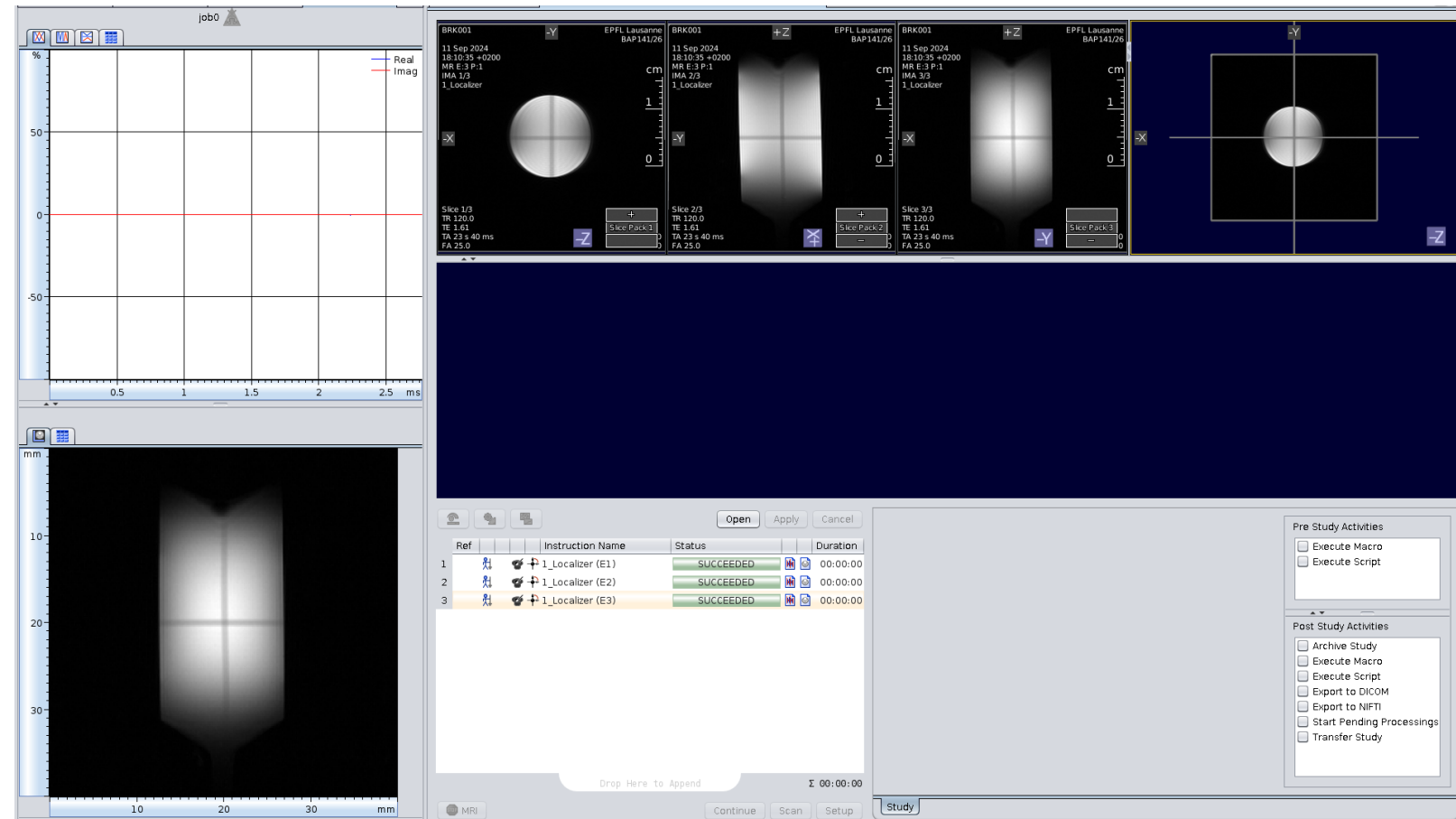
TUNING AND MATCHING

- Adjust resonant circuit such that:
 - It resonates at the Larmor frequency
 - Impedance matched to transmission line
- The dip must be at (or close to) 0 MHz.



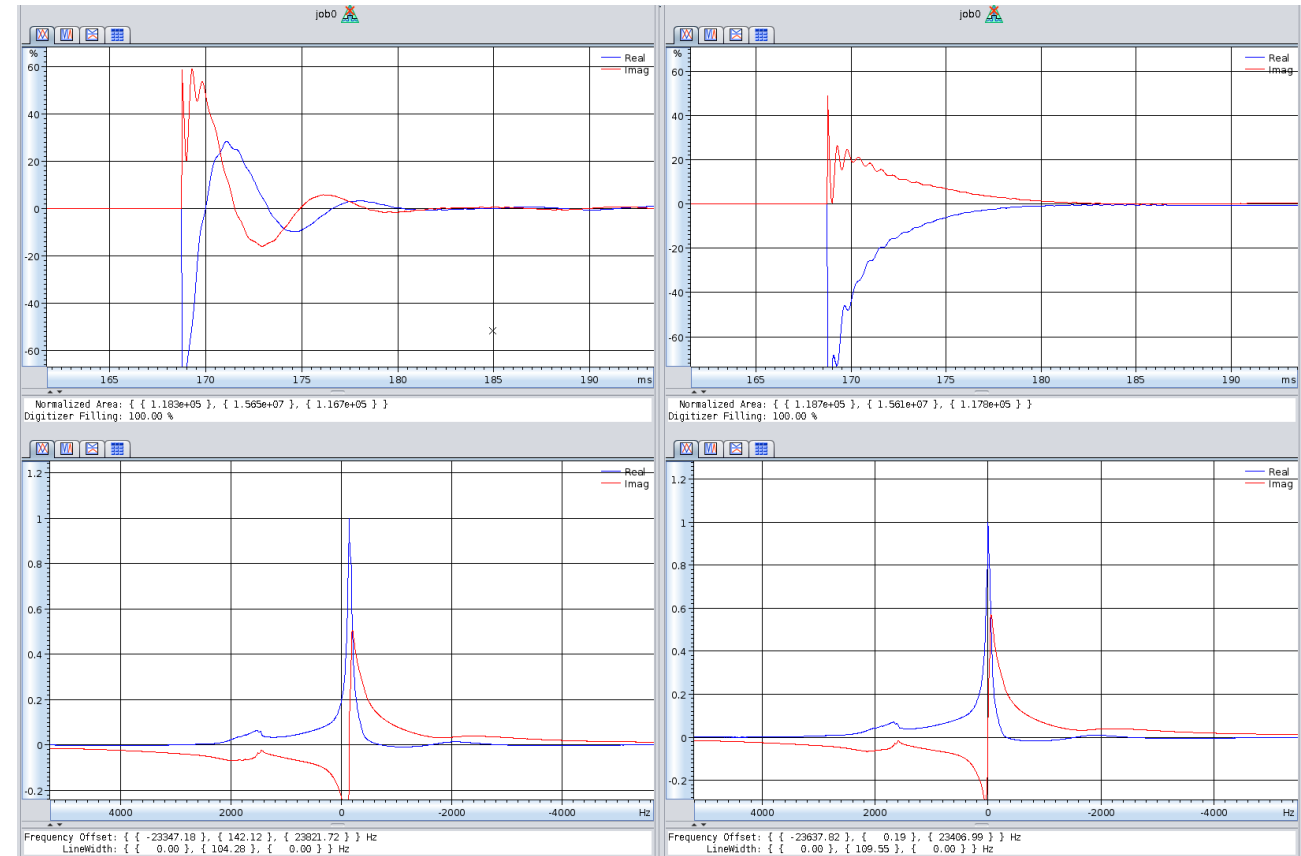
LOCALIZER

- We check that the sample is well centered.
- Otherwise we will need to move the slider.



FREQUENCY ADJUSTMENT

- Adjust the scanner's transmission/reception frequency to match the Larmor frequency of the sample.
- This sample resonates at 599.419141 MHz.
- When we are on resonance, the FID seen on the window stops oscillating, because we demodulate the signal with the exact same frequency.



Not adjusted

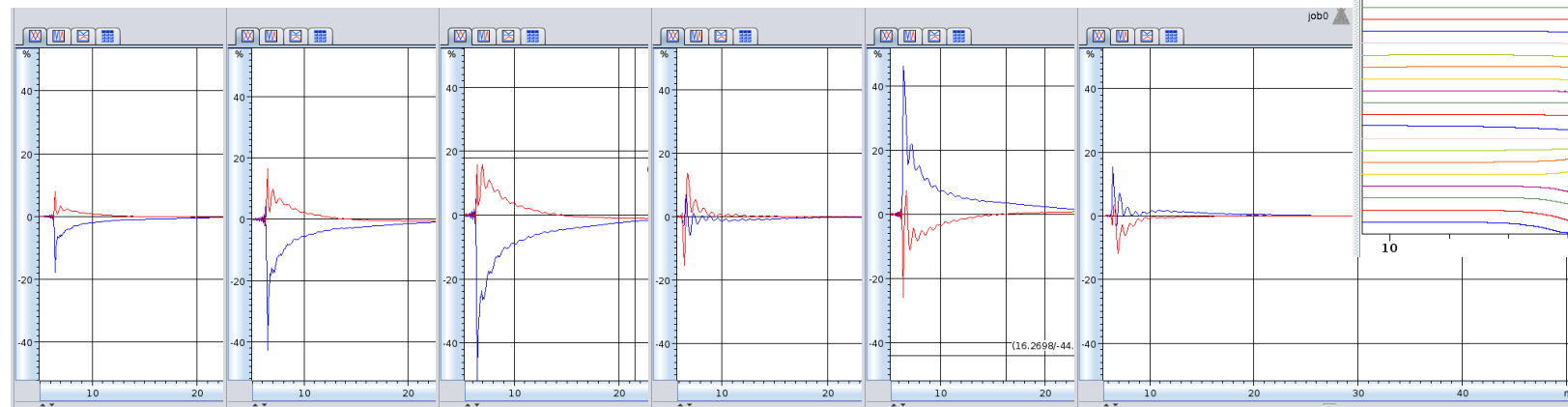
Adjusted

PULSE CALIBRATION

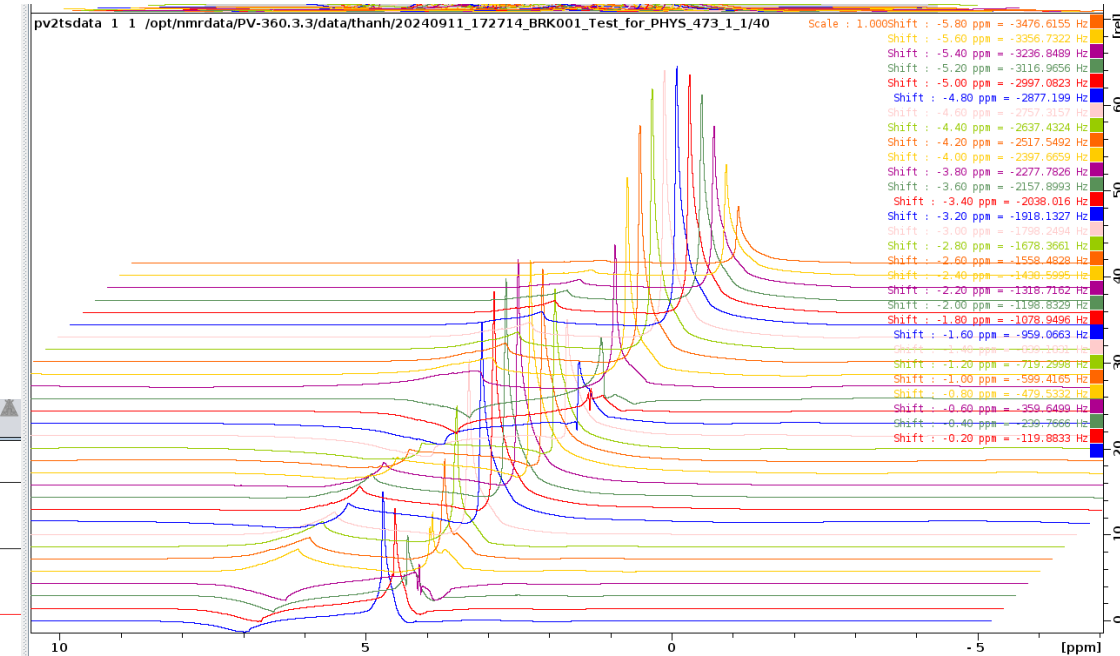
- Fixed power (10W), hard pulse
- Flip angle proportional to pulse length τ :

$$\alpha = \gamma \cdot B_1^+ \cdot \tau$$

- The maximum with 60us

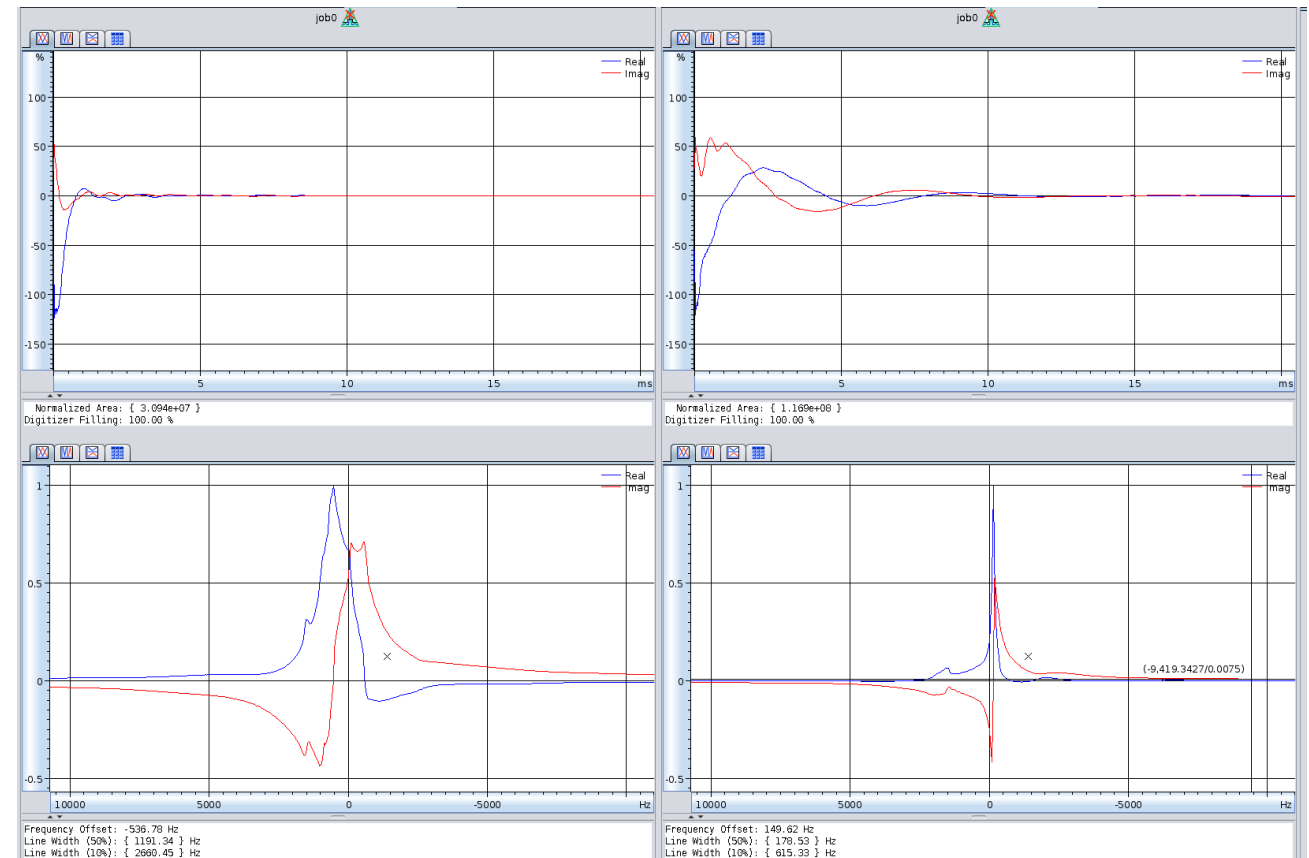


$\tau = 0.01\text{ms}$ 0.03ms 0.06ms 0.12ms 0.18ms 0.24ms



B₀ SHIMMING

- Compensate B₀ inhomogeneities by adjusting the current in the shim coils.
- The peak gets narrower, and FID decays more slowly.

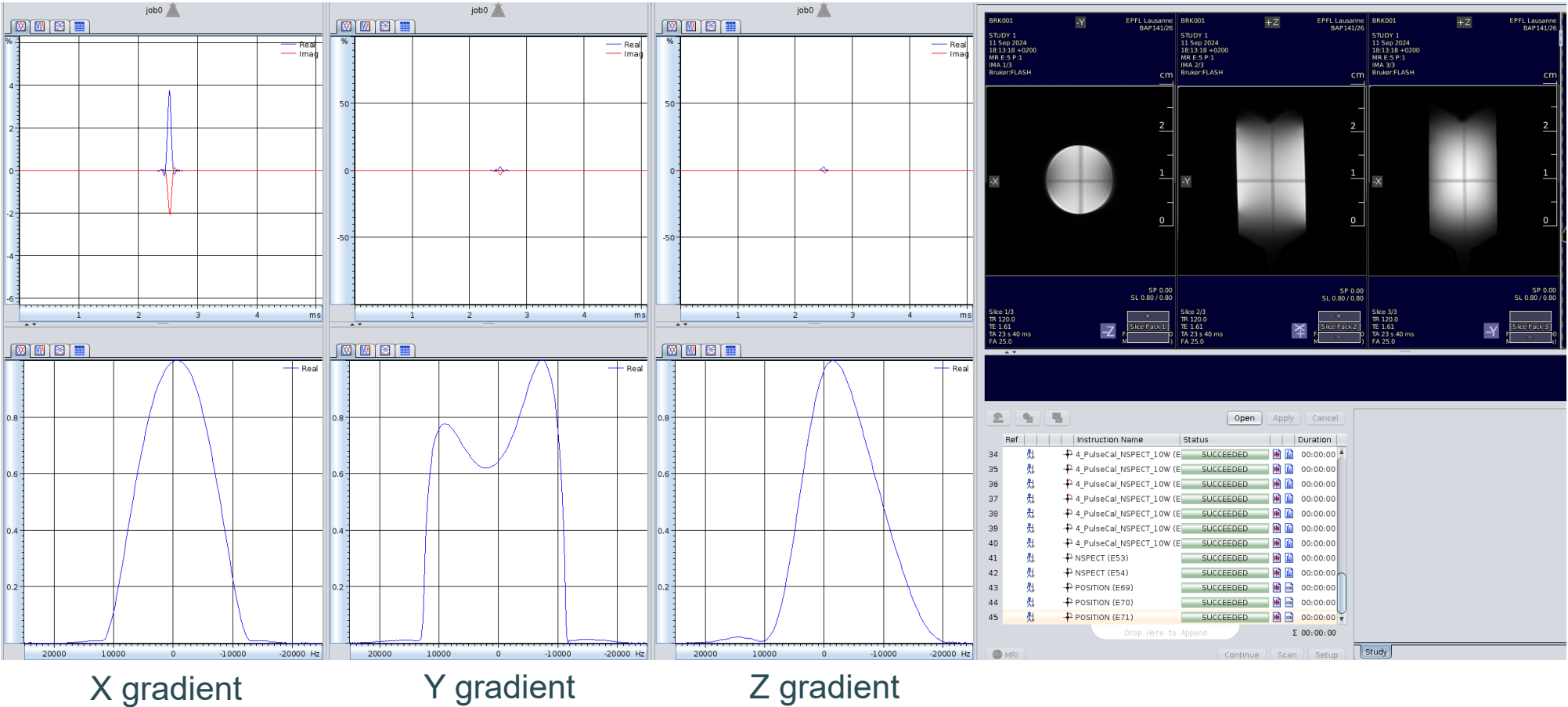


Unshimmed

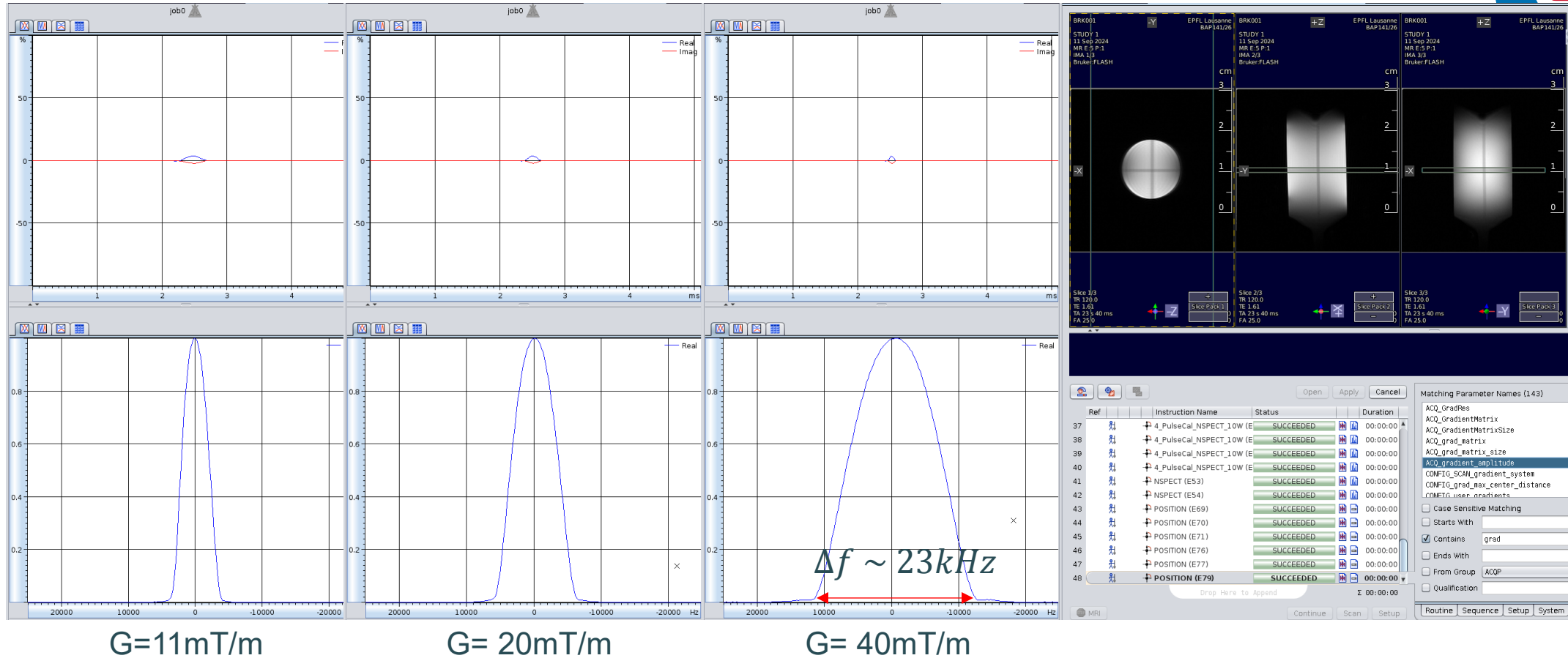
Linear shim

PROFILE 1D

- Frequency encoding using gradient on one axis at a time



PROFILE 1D (Y AXIS)

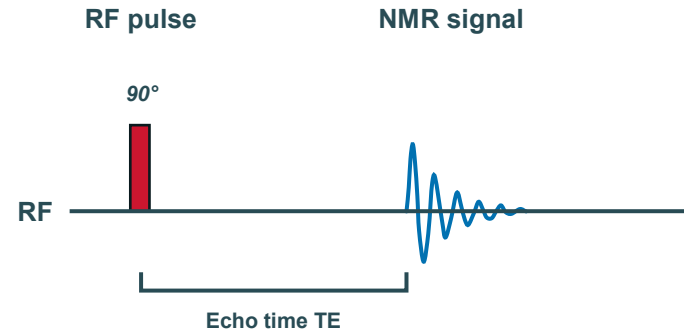


■ Could you calculate the syringe's diameter?

$$D = \frac{\Delta f}{\gamma_{1H} G}$$

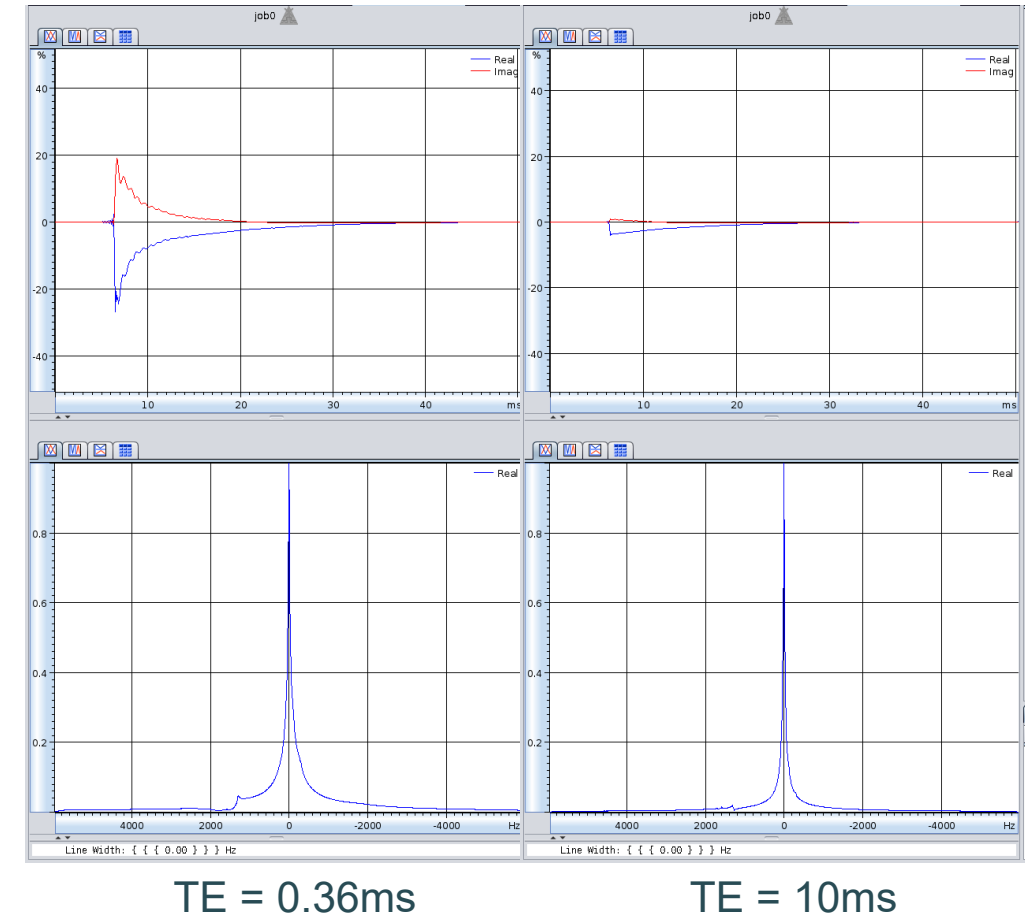
$\gamma_{1H} = 42.58 \text{ MHz/T}$

PULSE-ACQUIRE (NON-LOCALIZED GRADIENT-ECHO)

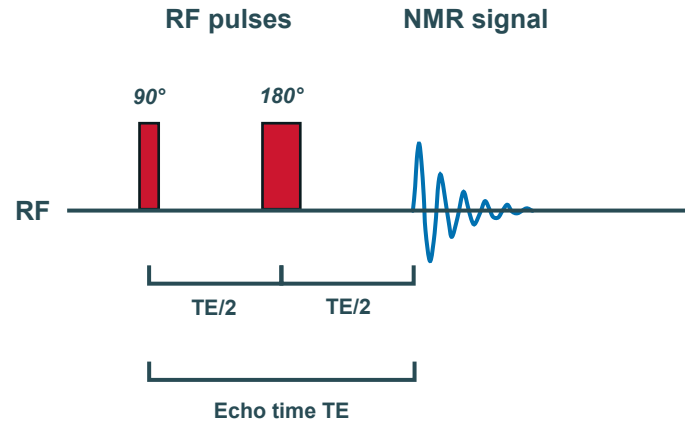


- Transverse magnetization evolves as:
$$M_{xy}(t) = M_0 (e^{-t/T_2^*})$$
- The echo time has a huge influence on the signal amplitude.
- To measure T_2^* , the experiment is repeated with different values of TE. The signal amplitude exponentially decays as a function of TE:

$$S \propto e^{-\frac{TE}{T_2^*}}$$



SPIN-ECHO (NON-LOCALIZED)



Transverse magnetization evolves as:

$$M_{xy}(t) = M_0 \left(e^{-t/T_2} \right)$$

- The echo time has a little influence on the signal amplitude.
- To measure T_2 , repeat with different values of TE. The signal amplitude decays as

$$S \propto e^{-\frac{TE}{T_2}}$$

